

- 1 The Validity and Reliability of the Rear Foot Elevated Split Squat 5RM to Determine
- 2 Unilateral Leg Strength Symmetry

3 Abstract

4 The purpose of this study was to examine the validity and reliability of the Rear Foot
5 Elevated Split Squat (RFESS) five repetition maximum (5RM) test as a field method
6 for measuring unilateral leg strength symmetry. As a validated method of testing
7 symmetry, the RFESS 5RM may be used by Strength and Conditioning coaches and
8 sports medicine staff to measure the presence of imbalances with minimal equipment
9 and time. 26 subjects (age = 23.8 ± 4.6 years, mass = 88.1 ± 10.7 kg, height =
10 1.79 ± 0.1 m) with a minimum two years strength and conditioning experience were
11 recruited. Following a familiarization session, subjects performed an incremental five
12 repetition maximum (5RM) protocol on both legs, on two occasions where 3D motion
13 and force data were collected. Moderate reliability of bar load symmetry was found
14 between test and re-test conditions correlation (ICC = 0.73, 0.33-0.91) with no
15 proportional bias between sessions. Validation of the exercise was analyzed using a
16 correlation between asymmetries in mean set vertical ground reaction forces (vGRF)
17 of the lead foot during the concentric phase, with bar load. When all maximal trials,
18 from both test conditions, were analyzed, a most likely large positive correlation (0.57,
19 0.30 to 0.76) were found for mean set concentric lead foot vGRF. When a threshold
20 level of load symmetry (96.54% - 103.46%) was applied, a most likely large positive
21 correlation ($r = 0.59$, 0.14-0.84) between symmetry in lead foot vGRF was found in
22 subjects who exceeded this limit. Conversely, analysis of subjects within the threshold
23 produced unclear correlations. Findings of this study suggest the RFESS is a valid
24 and reliable measure of unilateral leg strength symmetry. Practitioners are
25 recommended to use this exercise to investigate the strength symmetry of athletes,
26 but are guided to note that a threshold level of symmetry (96.54% - 103.46%) may be
27 required to have been exceeded to indicate a true difference in vGRF production.

28

29

30 Key Words:

31 Between-session; inter-limb differences; single leg; imbalances;

32 Introduction.

33 Lower limb strength symmetry is of interest to researchers, strength and conditioning
34 (S&C) coaches, physiotherapists and other sports medicine professionals, as there is
35 evidence to suggest that this may be linked to an increased risk of injury (22) and
36 reduced performance (25). However, the evidence pertaining to strength symmetry
37 and either reduced performance or increase injury risk is equivocal (11).
38 Consequently, a greater knowledge of symmetry and its interaction with both injury
39 and performance is required. Creating a more thorough understanding of the
40 implications of lower limb strength symmetry in athletes would provide clearer
41 guidance to inform S&C coaches. If an S&C coach can identify an athlete with a
42 strength imbalance between limbs, more informed decisions may be made about
43 possible performance deficits and risk to injury. Subsequently, training interventions,
44 for such an athlete, may be individualized to better mitigate these risks and further
45 enhance performance. However, for S&C coaches to respond to a lack of symmetry
46 there must be valid, reliable and practical method for collecting such data.

47 Previous research into strength symmetry has utilized direct methods of force
48 measurement, such as isokinetic dynamometry (ID) and force plates protocols. ID
49 techniques have been proven to be valid and reliable measures of unilateral strength
50 for knee flexion and extension (ICC's 0.88 – 0.98) and hip flexion and extension (ICC's
51 0.75-0.95) (1). Alternatively, force plate protocols have measured vertical ground
52 reaction forces (vGRF) through isometric actions such as the isometric mid-thigh pull
53 (IMTP) or back squat and in dynamic actions including the back squat (14) and Rear
54 foot elevated split squat (RFESS) (8). However, assessments which require either ID
55 or force plates maybe impractical in the time taken to conduct this analysis, require
56 additional financial costs, (in excess of that which is required to train an athlete) and

57 require specific expertise to operate. As such using ID or force plate protocols may not
58 provide a practical approach for coaches, in field settings, to collect symmetry data.

59 Assessment of differences in load, moved during closed kinetic chain exercises,
60 maybe a more accessible option to S&C coaches. Such exercises require no
61 additional equipment, except for those needed to perform the exercise (barbell and
62 plates). Under these conditions the bar load maybe considered a proxy measure of
63 force production. With respect to measuring strength symmetry this may only be
64 performed using unilateral exercises to determine the strength of each limb
65 independently. As such, S&C coaches may consider an axially loaded, closed kinetic
66 chain, dynamic exercise, such as the RFESS as one possible method of measuring
67 leg strength symmetry in athletes (10). Additionally, such an exercise should be
68 correlated to the performance of the athletes, as asymmetries are highly task
69 dependent (17, 23)

70 McCurdy et al., (21) and McCurdy and Langford (20) have previously reported the
71 RFESS as a reliable measure of unilateral leg strength (1RM ICC, 0.97- 0.99). The
72 study by McCurdy et al., (21) reported mean 3RM values of $98.6\text{kg} \pm 21.5\text{kg}$ and 1RM
73 $103\text{kg} \pm 21.5\text{kg}$ for the RFESS. When normalized to body mass, these were equivalent
74 to 1.12 kg/kg and 1.17kg/kg . To contextualize this data, Baker and Newton (4) reported
75 1RM bilateral back squat values of 1.78 kg/kg for elite Rugby League players. When
76 the unilateral strength data reported by McCurdy et al., (21) is compared to bilateral
77 data from Baker and Newton (4) the RFESS compares favorably. The relative load for
78 the unilateral exercise was greater than 50% of an equivalent bilateral exercise.
79 DeForest et al., (14) performed a kinetic comparison of two unilateral closed kinetic
80 chain exercises (Split squat and RFESS), in comparison to the back squat. The study
81 used a single force plate for all exercises, placed under the dominant foot of each

82 subject. No significant differences in peak vGRF were found between the back squat
83 (1414.8 ± 251.0 N) and RFESS (1412.3 ± 258.6 N). The split squat produced
84 significantly lower peak vGRF (1198.6 ± 187.9 N, $p < 0.05$). Whilst the force output from
85 the non-dominant limb or rear foot data was collected, this study does indicate that the
86 RFESS is comparable the back squat for peak force production. No rear foot data was
87 collected for either the split squat or RFESS, which is a key limitation to their findings.
88 Further research is required into the force production of the rear foot in the RFESS, to
89 better understand the role of each limb in performing this exercise.

90 Research into the RFESS indicates that it is kinetically comparable to the back squat
91 (14) and is a reliable method for measuring leg strength, through bar load (20, 21), in
92 different populations. Speirs et al (26), reported parity of improvements in 1RM back
93 squat, 1RM RFESS, speed and change of direction ability, when using RFESS or
94 back squat trained groups. However, no research, to date has validated this exercise
95 as a method for determining leg strength asymmetries, nor has any strength measure
96 been investigated for between session reliability. The hypothesis of this study is that
97 the RFESS is a valid measure of unilateral leg strength symmetry. Therefore, the
98 purpose of this study is to examine the validity of using the RFESS 5RM bar load to
99 measure leg strength symmetry and the between sessions reliability of the observed
100 imbalances.

101 METHODS.

102 Experimental Approach to the Problem

103 A between day repeated measures design was used to assess the validity and
104 reliability of the RFESS as a measure of lower limb symmetry. 26 male subjects
105 reported to the laboratory on three occasions to complete familiarization and testing.

106 Previous research has demonstrated a learning effect for the RFESS (21), therefore
107 visit one was a familiarization session and five repetition maximum (5RM) testing was
108 conducted on visits two and three to the laboratory. Force plates (Kistler 9827C, Kistler
109 Group, Winterthur, Switzerland) were placed under the lead and elevated rear foot, 10
110 Opus cameras recorded bar and joint position through 3D motion capture (Qualysis
111 AB, Gothenburg, Sweden). Reliability was determined by ICC and Bland-Altman
112 analysis of the symmetries in load achieved between test and re-test conditions. To
113 validate the RFESS 5RM as a test of symmetry, Pearson product moment correlation,
114 (PPMC) between asymmetries in both bar load and the set mean vGRF of the lead
115 foot (the mean of mean vGRF from all 5 repetitions per set) was performed on all
116 maximal trials.

117 Subjects

118 With institutional ethical approval, 26 male volunteers were recruited, (age = 23.8 ± 4.6
119 years, mass = 88.1 ± 10.7 kg, height = 1.79 ± 0.1 m). All subjects were engaged in a
120 structured S&C program including both bilateral and unilateral exercise and had at
121 least two years supervised training experience. Subjects were excluded from the study
122 if they have experienced a lower limb injury within the previous six months or have
123 had an injury requiring surgery to either limb previously. Of the 26 subjects, who
124 completed the first test condition, nine were unable to meet the re-test condition, due
125 to logistical constraints. These subjects were excluded from all further analysis of
126 reliability.

127 Procedures

128 Participation in this study required the subjects to attend a testing facility on three
129 occasions. The first were to perform basic anthropometric measures and

130 familiarization with the exercise protocol and the reserve rating of perceived exertion
131 (RIR-RPE) (28). The second and third visits required the subjects to perform an
132 incremental RFESS 5RM test on both limbs. The subjects were instructed to wear
133 appropriate sports footwear, which were consistent across all trials.

134 The procedure for testing the RFESS was adapted from DeForest et al., (14). The
135 subjects were positioned with their lead foot on the force platform, under their hips with
136 the rear foot elevated behind them where their toes were placed on the force plate,
137 elevated to 40cm (Figure 2).

138

139

140 ***INSERT FIGURE 1 ABOUT HERE***

141

142 The test was concluded, on each limb, when the athlete did not successfully complete
143 five repetitions of an assigned load. The subjects performed each incremental load
144 with alternating limbs first, to avoid bias and possible learning effects due to the cross-
145 education effect (19), achieving the maximal load within five trials. A successful trial
146 was deemed as performing five continuous repetitions with safe and effective
147 technique, within a 30s data collection window. Effective technique was considered to
148 be;

- 149
- 150 • Subject maintained balance throughout the exercise,
 - 151 • The heel of the front foot maintained contact with the ground throughout the
152 exercise.
 - 152 • Only the toe of the shoes of the rear foot were in contact with the force plate

- 153 • The subject maintained a neutral posture, and hip angle of approximately 180°,
154 from the rear leg.
- 155 • The knee of the rear limb descended below the height of the lead limb knee
156 and achieved a depth approximately equal to the height of the ankle on the lead
157 limb.

158 If a subject adopted a bilateral stance at any point within the trial or paused longer
159 than two seconds between repetitions, the trial was considered unsuccessful. The load
160 increments ranged from 1kg – 50kg, using International Weightlifting Federation (IWF)
161 accredited discs (Eleiko, Sweden). During data collection, immediate feedback of
162 Mean concentric velocity (MCV) was collected using a PUSH band (PUSH Inc.,
163 Toronto, Canada) wearable device on the dominant forearm of the subject, equidistant
164 from the wrist and elbow. Data was transferred to the PUSH™ App, via an iPad (Apple,
165 San Francisco, CA USA). Following each submaximal trial, the participants RIR-RPE
166 value (15, 28) and MCV of fifth repetition was used re-calculate the predicted maximal
167 load. The estimation of maximal load was firstly calculated using the trend line reported
168 by Carroll et al., (12) from barbell velocities observed during back squats of increasing
169 intensities. For the purpose of this study, only the velocity of the 5th repetition was used
170 to calculate estimated load. The final repetition was chosen as this represented the
171 maximal effort of the subjects, for that set. A second calculation was performed using
172 the RIR-RPE value to indicate the percentage of maximum effort. For example, an
173 RPE value of 7 indicated 70% of predicted 5RM load. Where there was disagreement
174 between the calculations for the predicted load, the lower of the two values was used.

175

176 The subjects were deemed to have achieved a maximal successful attempt when all
177 five repetitions were completed, the MCV of the fifth repetition was less than or equal
178 to 0.28 m/s (12) and declared an RPE of 9.5 or greater (28). Where only one of these
179 conditions were met, further increments were attempted until the subject achieved
180 these criteria or was unable to successfully perform the following increment.

181 Data Processing

182 During all trials, motion was captured through Qualysis Track Manager System at
183 250Hz (Qualysis AB, Gothenburg, Sweden) using 10 cameras (6 ceiling mounted and
184 4 floor mounted). During trials two and three reflective markers were placed at either
185 the end of the barbell, in the medio-lateral plane. Kinetic data was recorded from two
186 independent Kistler 9827C force plates at 1000Hz (Kistler Group, Winterthur,
187 Switzerland), the first being integral with the floor under the lead foot, the second
188 mounted on weightlifting blocks, under the rear foot.

189 Data was extracted and input into Microsoft Excel (Microsoft Corporation, Redmond,
190 WA, USA) and placed in a fourth order low pass Butterworth filter, using Biomechanics
191 toolbar, (27). All further data processing and analysis was performed using R (24),
192 with a code written specifically for this study. The initiation of a repetition was defined
193 as five consecutive increases in the magnitude of negative vertical bar displacement
194 and terminating at the time frame where five consecutive decreases in positive vertical
195 bar displacement occurred. This analysis was performed on the kinematic data taken
196 from 3D motion capture at 250Hz, representing 0.02s. Within each repetition the
197 eccentric and concentric phase were considered to end and start respectively at the
198 time point where maximal negative vertical bar displacement occurs. MCV was
199 calculated as the mean of all instantaneous velocities from the onset of the concentric
200 phase to the end of the repetition.

201 Analysis of symmetry validity was performed on two levels, firstly, across all maximal
202 trial data. Secondly, maximal data will be divided into more or less symmetrical
203 subjects, using equation 1. The application of a threshold level of detectable symmetry
204 was required, as a consequence of the interval nature of using free weight based
205 loads. Using force plates to precisely measure vGRF, as in the IMTP, reduces the
206 probability that a subject will produce the exact same force on both legs. As a result,
207 these methods of measuring leg strength are unlikely to find symmetrical subjects.
208 However, the use of weight plates restricts the sensitivity of load measurements, and
209 therefore increasing the possibility of producing a symmetrical finding. Strength
210 measurements, using weight plates, require the accurate prediction of the correct
211 increment which may successfully be performed by the subject. The smallest
212 increment possible is 1 kilogram, however, increments may typically be larger than
213 this. The predictive nature of this process is possible source of error. The application
214 of both MCV values and RIR-RPE scales, to predict the possible maximal load were
215 applied to mitigate against this risk. Furthermore, should a subject perform a maximal
216 load on one limb it may serve as an aspirational goal. This could potentially increase
217 motivation to achieve the same load on the contralateral limb, despite this possibly
218 being supra maximal for said limb, increasing the probability of producing a
219 symmetrical outcome.

220 *Equation 1: Symmetry threshold calculation*

221 *Symmetry threshold = (Mean load asymmetry – 100) + (1.64 + Standard Error of the*
222 *Mean).*

223

224 The identification and application of a load threshold, for symmetry measures, allows
225 the S&C coach to more accurately determine the true symmetry of their athletes, in
226 this test. As a consequence of the need for such a threshold a second analysis of
227 validity was performed on all maximal trials. Subjects were classified as either more
228 or less symmetrical using the following equation, adapted from Araújo et al., (2).

229 Symmetry Calculation

230 Bishop et al., (7-9), have reported the different methods of calculating asymmetries
231 from previous research. These reviews indicate the variance in outcomes between
232 calculations from a standardized data set. Further to this, the reviews justify a
233 difference in approach when using either a unilateral or bilateral exercise. It is
234 suggested that a singular approach is adopted for all unilateral and bilateral tests,
235 respectively. In keeping with this analysis and recommendation, the percentage
236 difference method (9) was used to calculate symmetry of all variables, using equation
237 1. Data is reported as a score of symmetry which is denoted by 100%, less than 100
238 indicates the left limb achieved a greater score than the right, conversely greater than
239 100, the right performed better.

240 *Equation 2: modified percentage difference method of calculating asymmetry, Bishop*
241 *et al., (9)*

$$242 \left(\frac{100}{(\max \text{ value}) - (\min \text{ value})} \times (-1) + 100 \right) \text{IF}(\text{left} < \text{right}, 1, -1) + 100$$

243 Statistical Analyses

244 Inter-test reliability, between tests one and two, was determined using PPMC the level
245 of reliability between tests was assessed using Intra class coefficient, (ICC), and
246 proportional bias between tests through a Bland-Altman test. The reliability, as
247 determined by ICC analysis, was classified according to following criteria; less than

248 0.5, poor, between 0.5 and 0.75 moderate, between 0.75 and 0.9 good , and greater
249 than 0.90 excellent (18) ICC values was reported with 95% confidence limits. If data
250 were not found to be normally distributed, it was log transformed before any further
251 analysis was completed.

252

253 All maximal trials from both sessions were used to analyze the validity of the 5RM
254 RFESS as a measure of leg strength symmetry. Set mean concentric vGRF was used
255 to determine the validity of the test. This value represents the mean of each of the five
256 repetitions mean concentric vGRF, for the set. In line with previous research, (3, 5, 6)
257 validity was determined by the PPMC between bar load and set mean vGRF
258 production, of the lead foot as well as the total set mean concentric vGRF of both
259 limbs. A second assessment of validity was performed on the two sub-groups
260 (asymmetrical and symmetrical). PPMC values was classified according to Cohen's
261 effect sizes (13), using the following criteria: trivial (0.1), small (0.1–0.3), moderate
262 (0.3–0.5), large (0.5–0.7), very large (0.7–0.9), or practically perfect (.0.9). A
263 magnitude-based inferences approach was adopted to report findings. Cohen (13)
264 identified an r value of 0.1 as the smallest clinically important correlation, therefore this
265 was set as threshold of analysis for inferences in all correlational analysis. The
266 magnitude based inferences were analyzed, based on the probability that the
267 correlation observed was greater than 0.1 and classified as follows; <0.5% almost
268 certainly not; 0.5-5% very unlikely; 5-25% unlikely; 25-75% possibly; 75-95% likely;
269 95-99.5% very likely; >99.5% almost certainly, where there is greater than 5% chance
270 of both a negative and positive result, the inference will be deemed unclear. (16).

271 RESULTS.

272 The mean bar load of all successful trials from both limbs and test conditions was
273 84kg \pm 16.8kg. When normalized to body mass, the loads achieved were 0.96 \pm 0.18
274 kg/kg. When bar loads were compared between test and re-test conditions a most
275 likely positive increase (9.3%) in bar load was observed. A most likely very large
276 positive correlation ($r = 0.93$, CL 0.88-0.96) and an excellent level of reliability was
277 found (ICC = 0.93 CL 0.88-0.96).

278

279 ***INSERT TABLE 1 ABOUT HERE***

280 ***INSERT TABLE 2 ABOUT HERE***

281

282

283 Using the equation (equation 2) presented previously, a symmetry threshold of
284 94.91% - 105.9% was set to differentiate between more and less symmetrical
285 subjects.

286 **Reliability analysis**

287 Analysis of symmetry, of bar load, found a most likely large positive correlation
288 between test conditions ($r = 0.73$, 0.33-0.91), (fig 1), and moderate reliability (ICC 0.73,
289 0.39-0.89). The symmetry observed in the initial test was 99.67 \pm 18.77% and 102.84
290 \pm 6.35% under re-test conditions, the standard error was 1.29% The Bland-Altman
291 analysis (fig 2) found a mean difference of 0.26, (-12.44-12.97), indicating no
292 proportional bias between testing days.

293

294

295 ***INSERT FIGURE 2 ABOUT HERE***

296

297 ***INSERT FIGURE 3 ABOUT HERE***

298 **Validity analysis**

299 The mean symmetry for bar load, for all maximal trials was $101.08\% \pm 10.13$, for the
300 same trials the symmetry in mean set concentric vGRF was $101.76 \pm 5.14\%$ (lead foot
301 only) and $101.84 \pm 4.33\%$ (lead and rear foot combined). Correlation analysis of
302 symmetry data, from mean vGRF, found a most likely large positive effect for both the
303 lead foot only and when lead and rear foot were combined. When normalized to body
304 weight, most likely large positive correlations were found for both lead foot vGRF and
305 lead and rear foot vGRF, respectively.

306 ***INSERT FIGURE 4 ABOUT HERE***

307 ***INSERT TABLE 4 ABOUT HERE***

308

309 When threshold boundaries of load symmetry (94.91% - 105.9%), were applied, those
310 subjects outside this range were found to have very likely large positive correlation
311 between asymmetries in lead foot vGRF and bar load. The same inference was also
312 found when lead foot vGRF was normalized to body weight. When vGRF of both front
313 and rear foot was combined a most likely very large positive correlation was found to
314 asymmetries in bar load. In the more symmetrical group, the correlation between

315 symmetry in mean vGRF of the lead limb and lead and rear limb combined, to that of
316 bar load, was found to be unclear.

317

318 DISCUSSION.

319 To date, this is the first study to investigate the reliability and validity of a field based,
320 free weight method of measuring unilateral leg strength symmetry. Findings of this
321 study demonstrate that the RFESS 5RM demonstrates both good validity and
322 moderate to excellent reliability. S&C coaches may consider using the RFESS 5RM
323 to determine leg strength symmetry.

324 Data from test and re-test conditions indicated a most likely very large positive
325 correlation between trials with moderate reliability (ICC= 0.73, 0.46-0.87) and no
326 proportional bias. The reliability of loads between trials in this study (ICC = 0.93) and
327 the loads achieved (84kg \pm 16.8kg) compare favorably to study previous research (21)
328 (ICC's >0.94, 3RM values 98.6kg \pm 21.5kg, 1RM 103kg \pm 21.5kg). This indicates that
329 the RFESS is a reliable measure of unilateral leg strength, when using 5, 3 or 1RM
330 protocols. However, McCurdy et al., (21) offered no data regarding the symmetry of
331 the subjects in their study. The current study is the only one, to date, to do so, finding
332 moderate reliability between sessions (ICC 0.73, 0.46-0.87). An increase in load was
333 observed between sessions of 9.3% indicating a most likely increase, which may
334 represent a learning effect between tests. Such an effect, which is larger than the
335 magnitude of asymmetry detected, may suggest that the reliability of the test is
336 questionable. The between session reliability of both load lifted and asymmetry
337 though suggests that the increase in strength between sessions did not affect this
338 imbalance and both limbs experienced equals gains. Further research, which

339 incorporates greater familiarization to the exercises may reduce the learning effect
340 between sessions and enhance the reliability of the test.

341 Koo et al., (18) recommends a sample size of 30 subjects to establish reliability using
342 an ICC analysis. As this study was limited to only 17 subjects, who completed test and
343 re-test conditions, the ability to meet the threshold for good reliability is less probable.
344 Therefore, expanding the sample size may further increase the probability and effect
345 size of the reliability between sessions. The sample, was relatively homogenous being
346 of similar age, gender and training experience. As demonstrated by the learning effect
347 in this study, participation in such a task required a minimum training status to limit
348 possible learning effects between tests. A larger sample size, with greater range of
349 training ages and exposure to the exercise may have also reduced the learning effect
350 reported in this study. The homogeneity of the sample, does restrict the applicability
351 of the findings to similar populations. Further research with either a larger, more
352 general sample or specific targeted groups, which may benefit from the test is
353 warranted.

354

355 Furthermore, the challenges of using weight plates to determine performance in the
356 tests further constrains the precision of the test. However, given these constraints the
357 level of reliability fell 0.02 from being classified as good. If the reliability of the load
358 scores are considered in conjunction with the marginal differentiation between
359 moderate and good reliability, S&C coaches may consider the RFESS 5RM to be a
360 reliable method of measuring leg strength symmetry.

361 The current study sought to use set mean vGRF data to validate the RFESS as the
362 first closed kinetic chain, dynamic, free weight exercise, to measure unilateral leg

363 strength symmetry. The RFESS requires vertical movement of an axially loaded mass,
364 in the sagittal plane, as such, the validity of symmetry in bar load is theoretically linked
365 to differences in set mean concentric vGRF between limbs. The use of PPMC to
366 analyze the relationship between symmetries in bar load and set mean concentric
367 vGRF was applied to determine the validity of the exercise. When all maximal trials,
368 from both test dates, were analyzed, symmetries in both lead foot and total (lead foot
369 + rear foot) set mean concentric vGRF were found to have most likely large positive
370 correlations. This suggests that the RFESS 5RM is a valid measure of unilateral leg
371 strength symmetry, as shown by the ability to produce set mean concentric vGRF.

372 However, the application of a symmetry threshold, polarized the correlation findings.
373 There were unclear findings in those subjects which fell within this boundary.
374 Conversely, subjects which exceeded the threshold boundary, demonstrated a most
375 likely large positive correlation between asymmetries in bar load and lead foot set
376 mean concentric vGRF. These findings further support the validity of the RFESS 5RM,
377 to measure symmetry in leg strength, but suggests that the test has a level of
378 sensitivity which is $\pm 5.09\%$, in this sample.

379 The data from this study supports the hypothesis that the RFESS 5RM is a valid and
380 reliable method of measuring unilateral leg strength symmetry, based on lead foot
381 vGRF data. However, whilst there is good evidence supporting the exercise based
382 on lead foot data, marginally stronger relationships were found between bar load
383 combined front and rear foot vGRF were found ($r = 0.53$ lead, 0.67 lead + rear foot).
384 The data from this study found that a mean of $84.41\% \pm 5.40$ of force was produced by
385 the lead foot during the exercises. However, when applying the effect size limits
386 recommended by Cohen (13), both these variables are classified as high and neither
387 resulted in a different magnitude based inference. The inability to draw different

388 inferences between these two variables may indicate that the role of the rear foot does
389 not perform a significant role in the concentric phase of this exercise. This conclusion
390 may be further supported by the low variability in (CV = 6.4%) in lead foot force
391 distribution across all maximal trials. Further research is required to better understand
392 the role of the rear foot in this exercise, specifically in relation to different submaximal
393 loads, to examine if the role of the rear limb changes with increasing intensity.

394 All subjects in this study had a minimum of two years structured resistance training
395 prior to data collection. However, none had previously performed the RFESS to
396 maximal level and reported different loading methods in previous training experience.
397 McCurdy et al., (21) reported significant changes ($p > 0.05$) in RFESS performance
398 between trials, indicating that a learning effect had taken place, which is in agreement
399 with the findings of this study. Despite the inter-test differences in loads, in this study,
400 the results were found to be reliable and no bias in symmetry was found. As a result,
401 the use of more experienced subjects may further increase the reliability observed in
402 this and similar studies but may not influence the symmetries found.

403 PRACTICAL APPLICATIONS.

404 The findings from the current study indicate that the RFESS is a reliable method of
405 determining unilateral leg strength in a field setting. Furthermore, when using the
406 percentage difference method of calculation, the asymmetries observed in bar load
407 are indicative of an athlete's symmetry in producing vGRF. From the sample used in
408 this study, a threshold boundary of symmetry was observed of $\pm 5.09\%$. The RFESS
409 5RM appears to lack sensitivity to symmetry below this level and therefore athletes
410 within this range may not be considered to be asymmetrical. S&C coaches may be
411 able to implement this protocol to both find a valid and reliable measure of their
412 athlete's leg strength and their degree of symmetry

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495 **Figures**496 *Figure 1: Demonstration of the configuration for data collection in the RFESS 5RM*

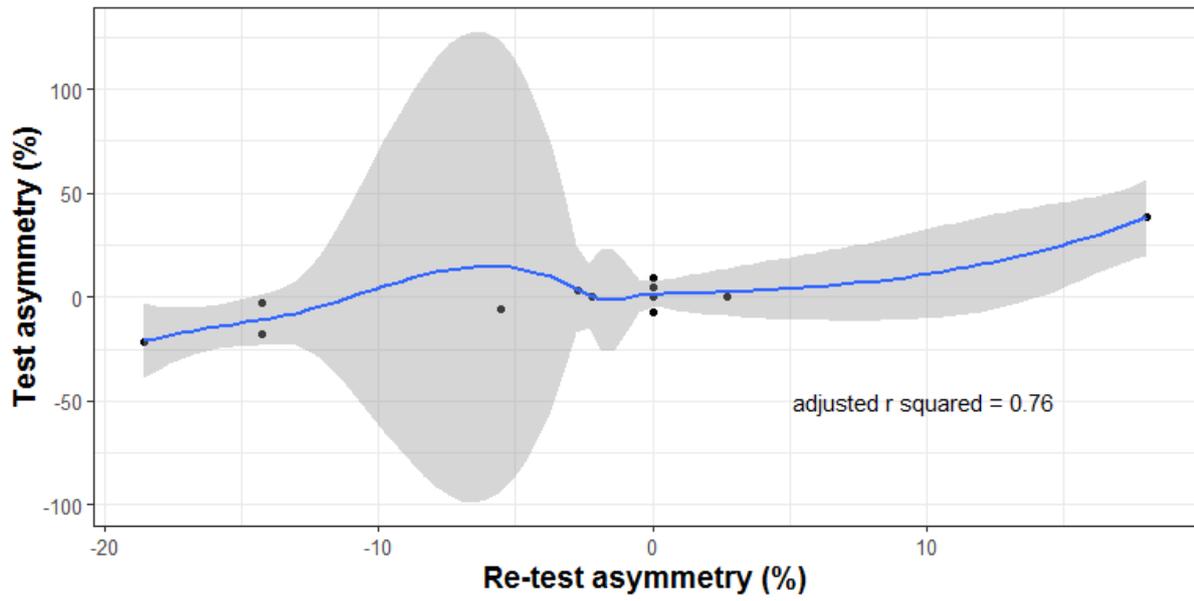
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498 *Figure 2: Scatter plot of test and re-test symmetry (%) in subjects performing a 5RM*

499 *RFESS*

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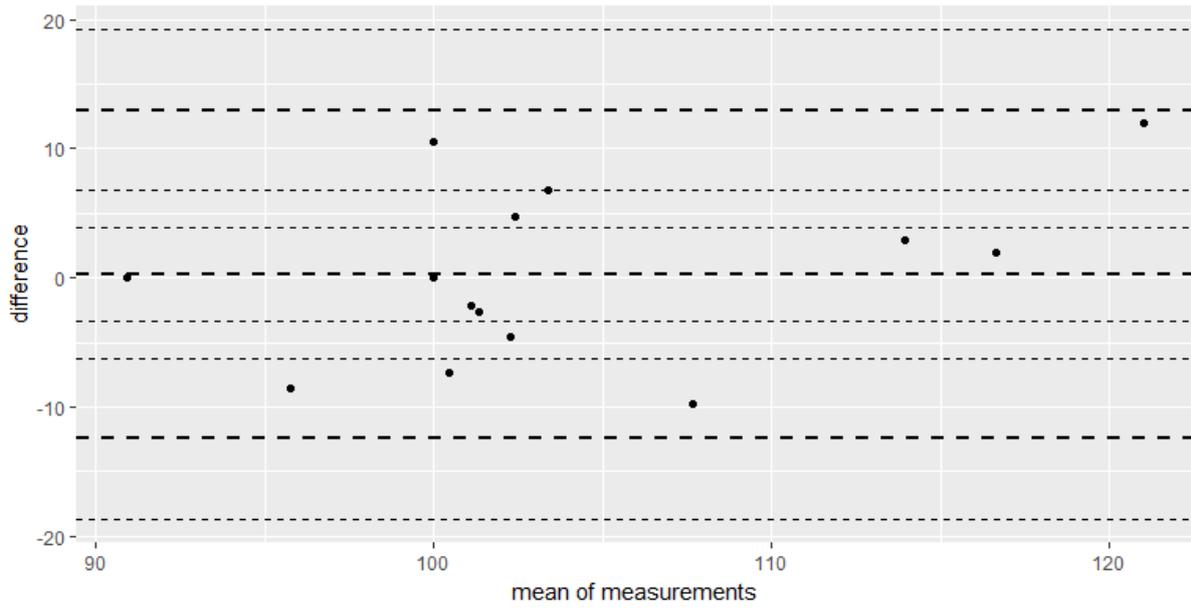
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504 *Figure 3: Bland-Altman plot of test and re-test symmetry (%) in subjects performing a*

505 *5RM RFESS*

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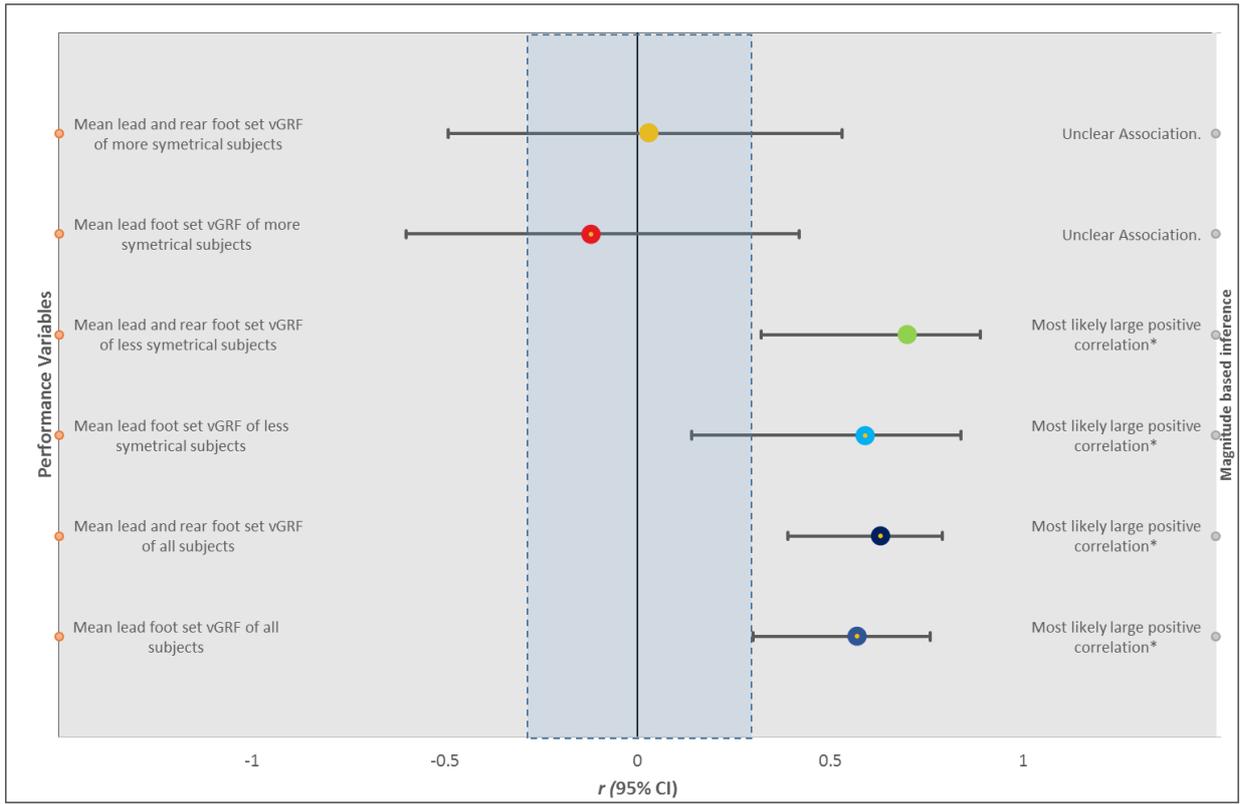
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512 Figure 4: Forest plot showing the correlation ($r + 95\%$ CL) between bar load and mean set vGRF
513 asymmetry in all, less and more symmetrical subjects.

514 • Significant $p = <0.05$



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517 Tables

518

519 *Table 1: Mean data for all successful trials of the RFESS 5RM, between different*

520 *trials.*

	Test		Re-test	
	Left	Right	Left	Right
Mean bar load (kg)	80.9±15.2	82.0±16.37	89.5±16.3	88.8±18.2
Mean bar load, normalised to body mass (kg/kg)	0.92±0.17	0.94±0.19	1.0±0.2	0.99±0.2

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523 *Table 2: Mean kinetic data from all maximal RFESS 5RM trials, pooled from both*
 524 *test and re-test conditions.*

	Mean (\pm SD)
Mean lead foot only vGRF (N)	1423.97 \pm 195.59
Mean lead foot only vGRF (BW)	1.64 \pm 0.23
Mean rear foot only vGRF (N)	266.79 \pm 80.60
Mean rear foot only vGRF (BW)	0.31 \pm 0.09
Mean lead and rear foot vGRF (N)	1700.95 \pm 246.20
Mean vertical Force (Lead and rear foot vGRF) (BW)	1.95 \pm 0.28
Mean vGRF Distribution toward the lead foot (%)	84.41 \pm 5.40

525

527 *Table 4: Magnitude based inference data from Pearson correlation analysis of mean vGRF and bar load symmetry*

Variable	r (95% CL)	Inference	% Positive	% Trivial	% Negative
Mean lead foot set vGRF of all subjects	0.57, (0.30 to 0.76)	Most likely large positive correlation*	99.90%	0.10%	0.00%
Mean lead and rear foot set vGRF of all subjects	0.63, (0.39 to 0.79)	Most likely large positive correlation*	100%	0.00%	0.00%
Mean lead foot set vGRF of less symmetrical subjects	0.59, (0.14 to 0.84)	Most likely large positive correlation*	98.10%	1.60%	0.30%
Mean lead and rear foot set vGRF of less symmetrical subjects	0.70, (0.32 to 0.89)	Most likely large positive correlation*	99.70%	0.30%	0.00%
Mean lead foot set vGRF of more symmetrical subjects	-0.12, (-0.60 to 0.42)	Unclear Association.	15.60%	30.70%	53.70%
Mean lead and rear foot set vGRF of more symmetrical subjects	0.03, (-0.49 to 0.53)	Unclear Association.	37.40%	35.10%	27.50%

